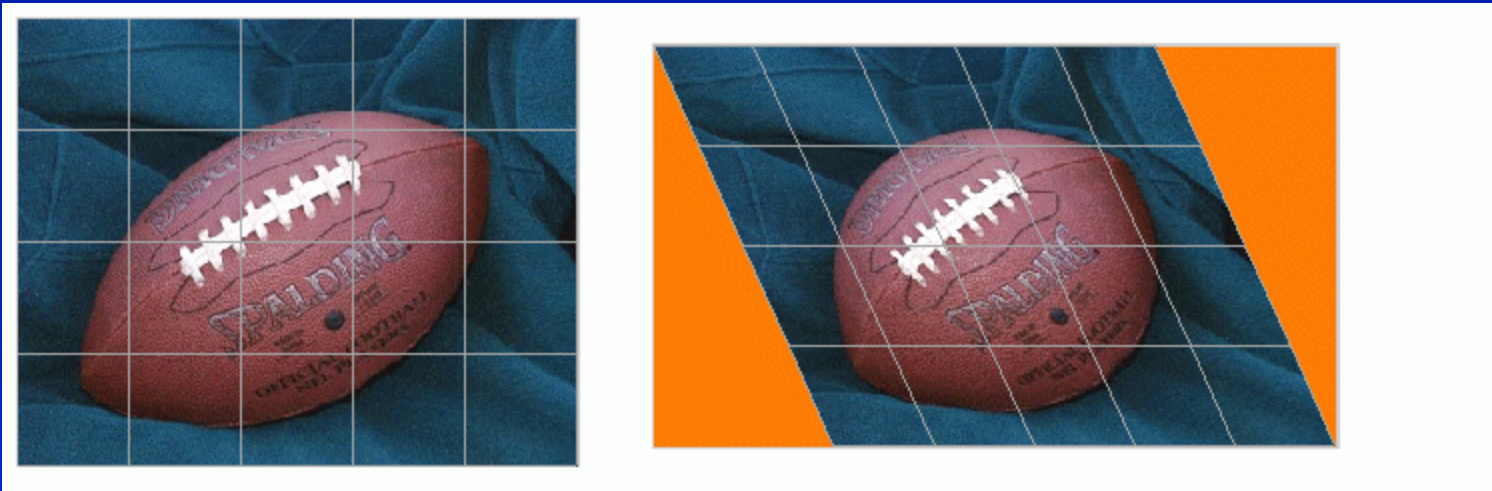


# Technical aspects of SPECT and SPECT-CT

John Buscombe



# What does the clinician need to know?

- *For SPECT*
  - What factors affect SPECT
  - How those factors should be sought
  - Looking for artefacts
- *For SPECT-CT*
  - Issues of registration

# Factors that effect SPECT

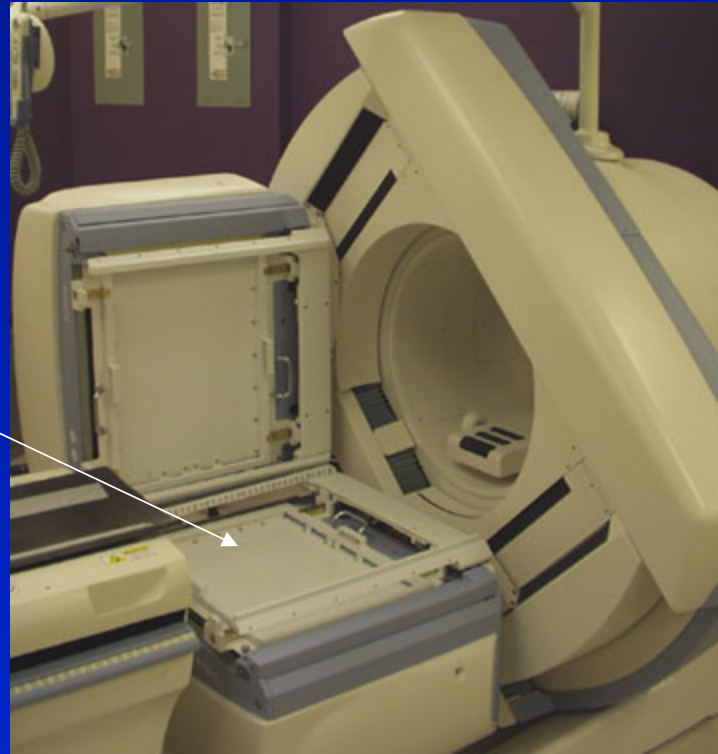
- *Uniformity*
  - CFOV <2.5% variation in uniformity (extrinsic)
  - Should be tested by flood source
  - Intrinsic uniformity done with point source and no collimator
- *Centre of rotation*
- *Linarity*
- *Energy correction maps (for different isotopes)*
- *Using the correct collimator*
- *SPECT resolution*

# Needs a QC programme

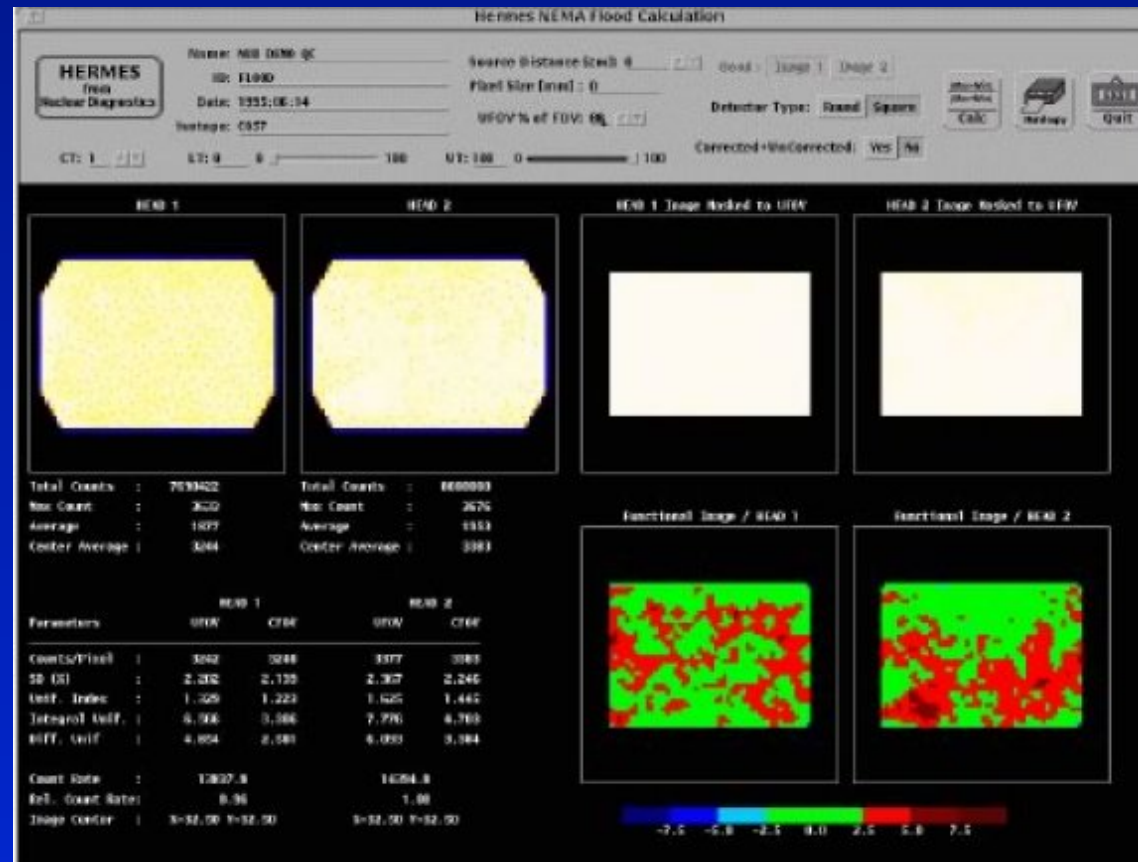
- *Typical programme*
- *Daily*
  - Flood for uniformity
- *Monthly*
  - COR
  - Linearity
- *3 Monthly*
  - Flood corrections for less used isotopes
  - Resolution

# Uniformity

**Note  
flood  
tank on  
gamma  
camera**



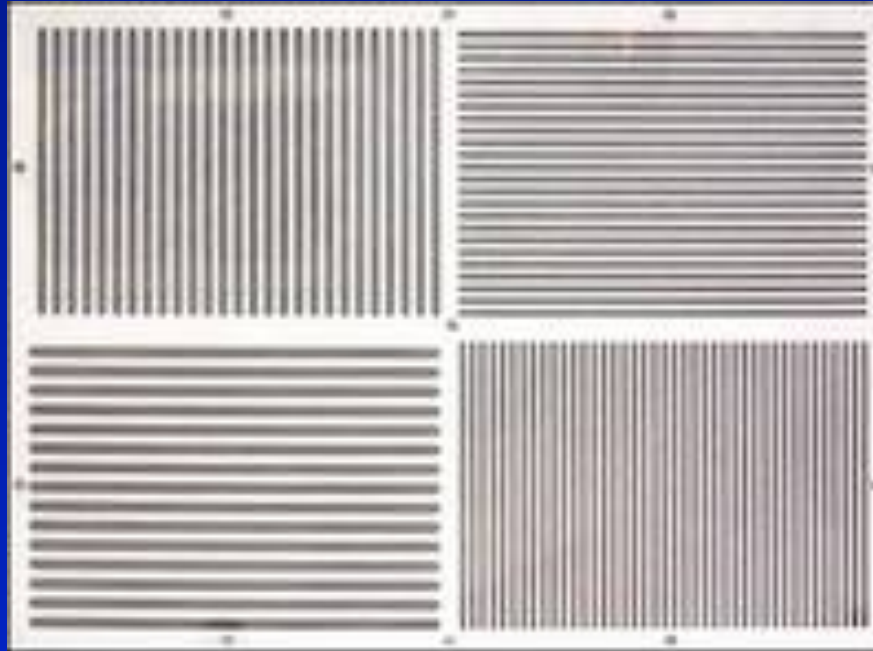
# Uniformity



What is wrong on this triple  
headed gamma camera?



# Linearity



**Tungsten cut out shield used with flood tank**



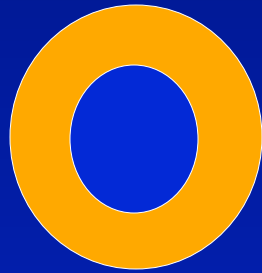
# COR

- *Use capillary tube of activity placed in the centre of rotation normally 10 cm long*
- *Acquire SPECT*
- *Reconstruct image*

# COR



**Perfect  
heads**

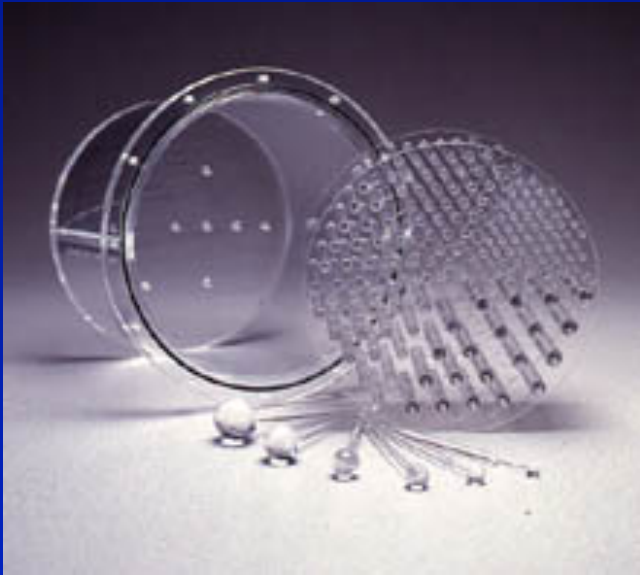


**single head poor COR**

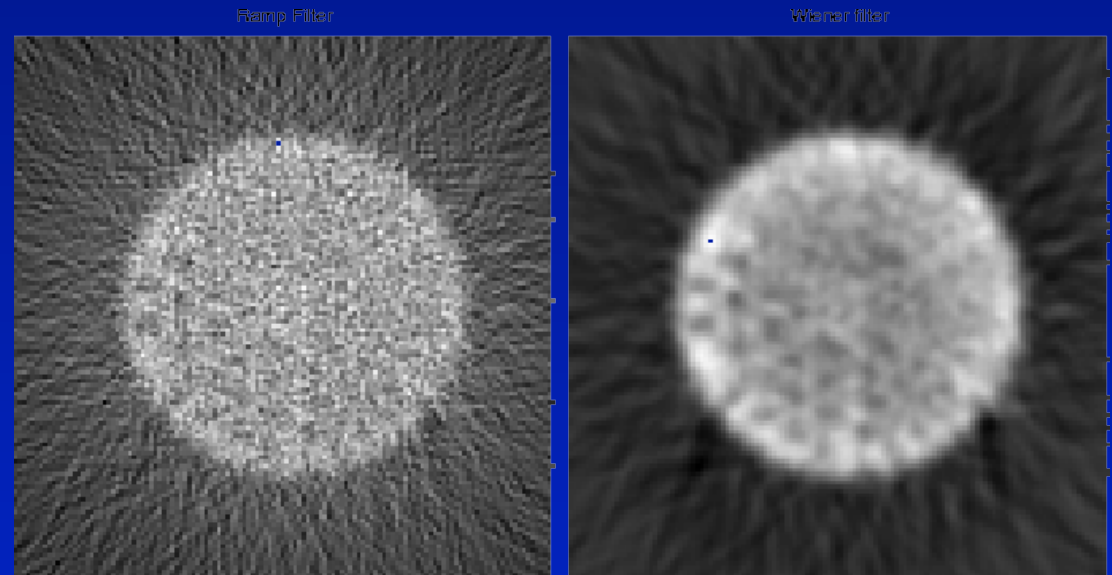


**2 heads both with  
good COR but  
misaligned**

# SPECT resolution



**Jaszack SPECT phantom**



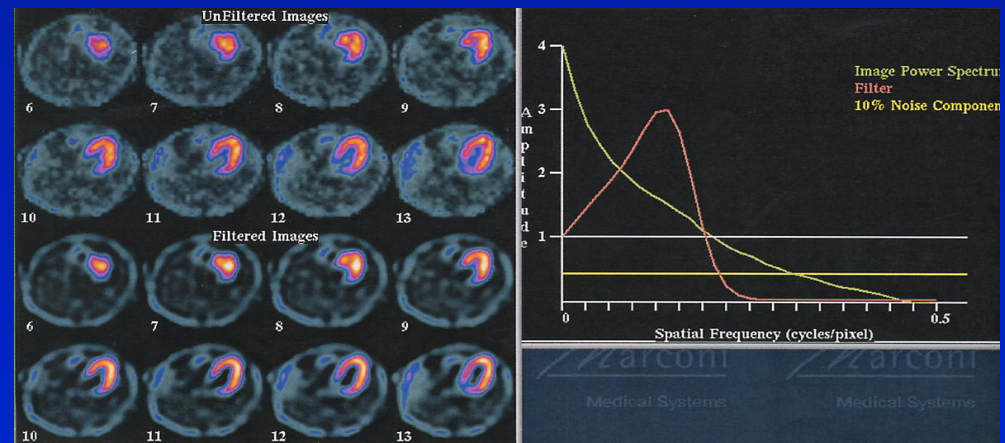
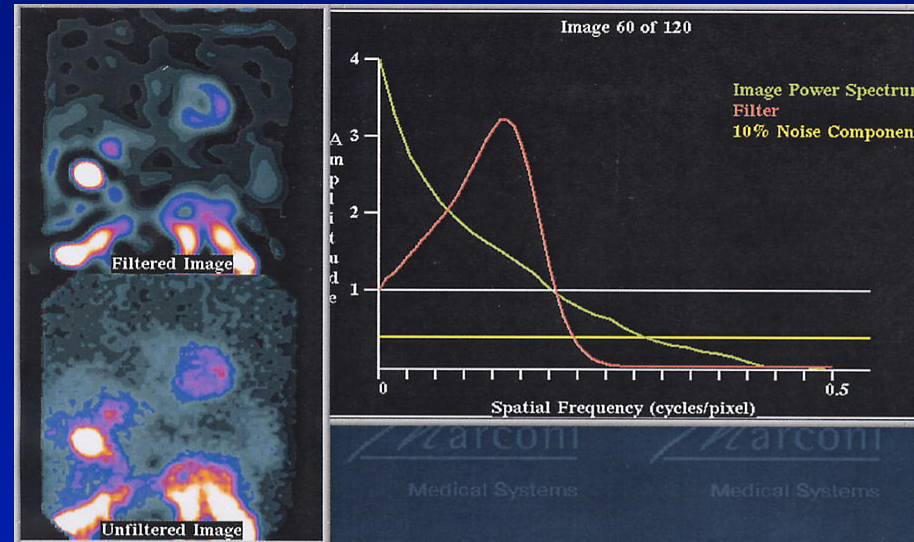
**Images (filtered and unfiltered)**

# Then all you need to do

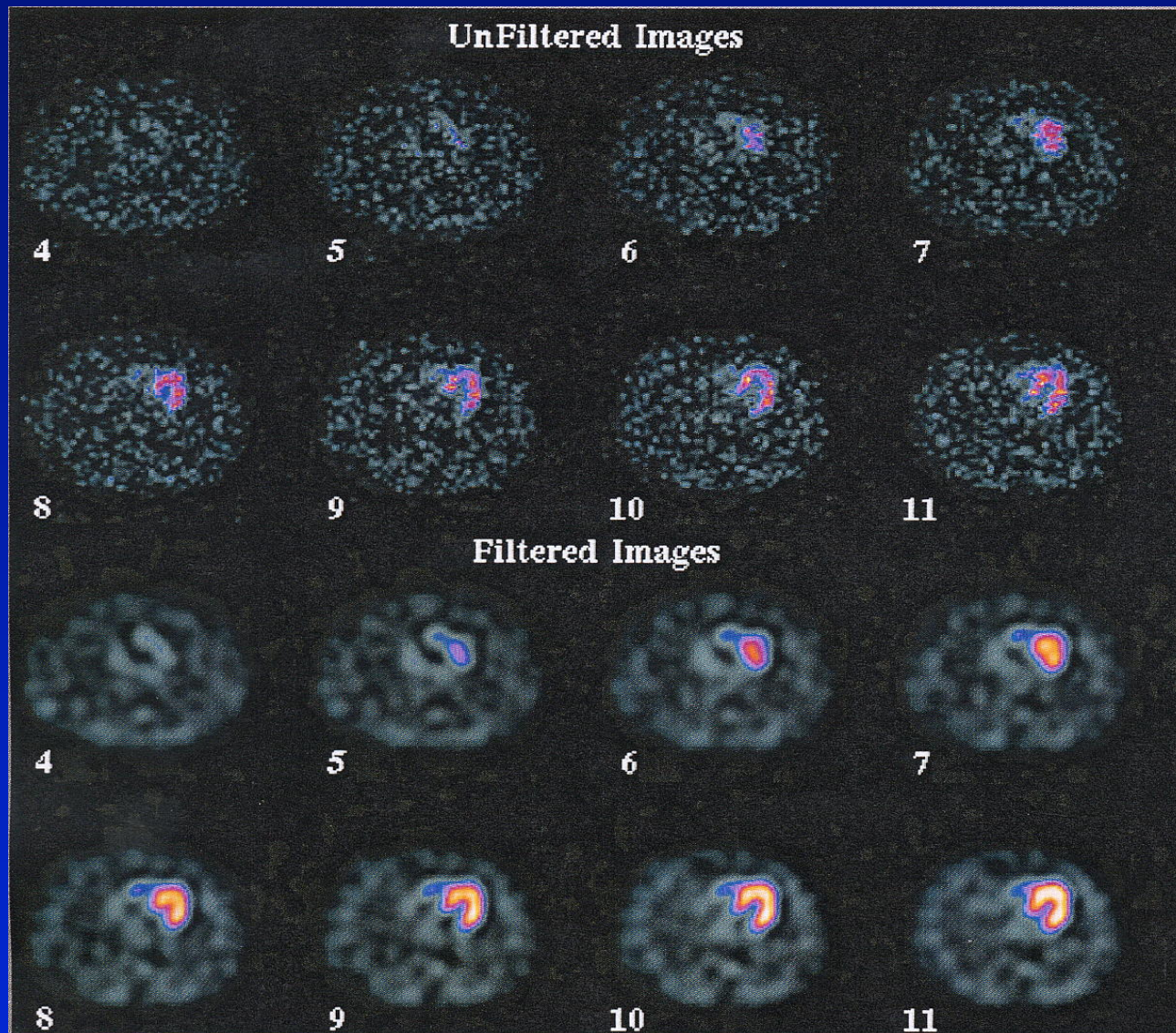
- *Reconstruct image correctly*
  - Back projection
  - Iterative
- *Correct filtering*
  - Some filters more count dependent than others
  - Though called the same different manufacturers filters often very different

# Filtering

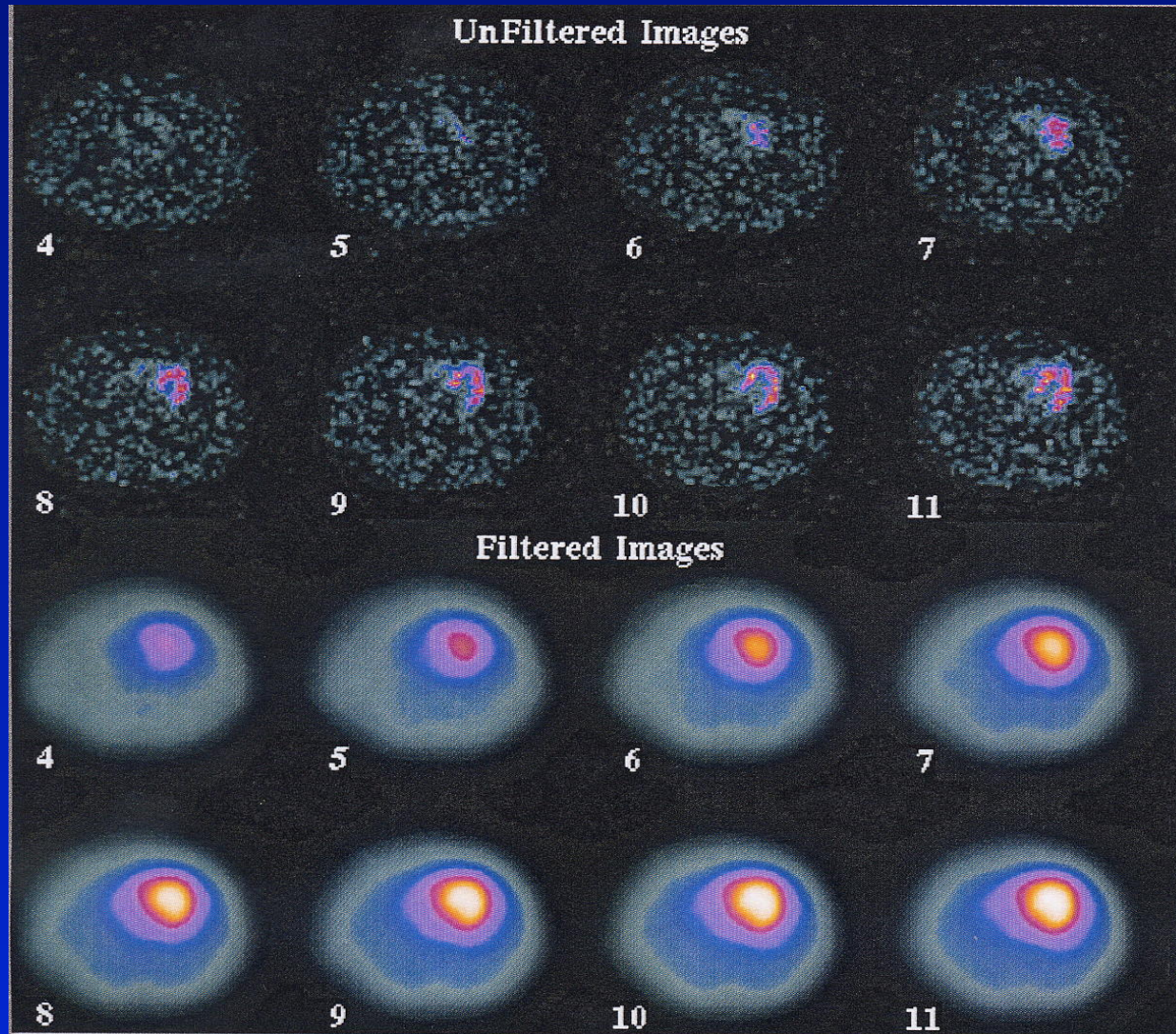
- *Can use predefined protocols*
- *However filter count related*
- *Maybe best to use a manual filter*
- *Check images are not over filtered*



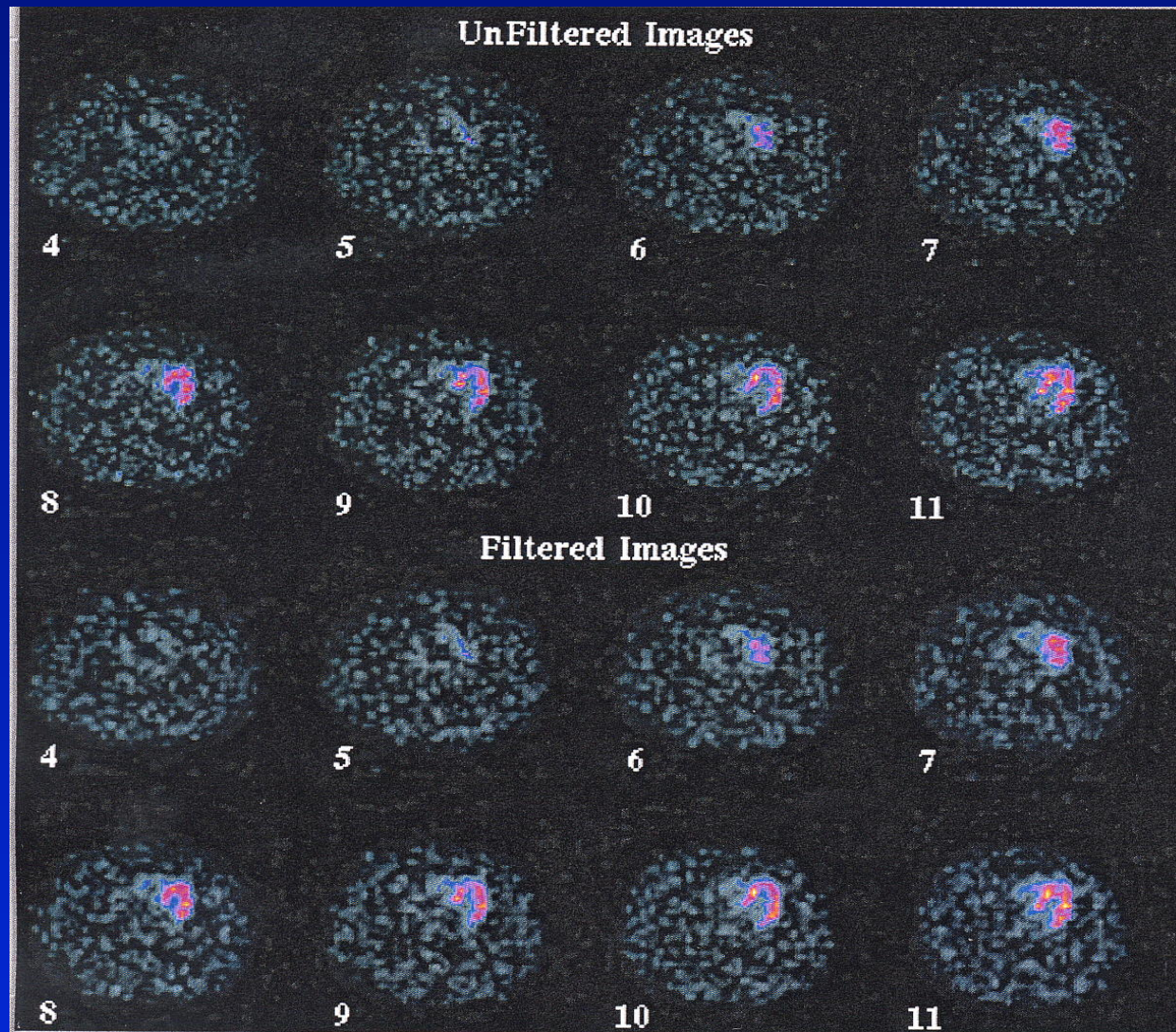
# Post filtering-correct



# Over smoothed



# Over filtered





# Image Fusion



# Image Registration

- Process of spatially aligning images from the same or matching modalities
- CT/MR/NM

# Image Registration

- Intra/Inter modality
- Two approaches
  - Dedicated dual modality hardware
  - Software algorithms

# Why?

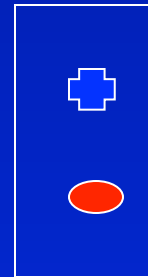
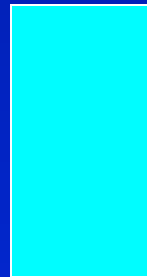
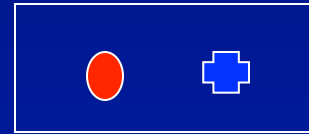
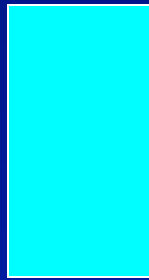
Allows:

- Fusion of molecular and anatomical information
- Maximise potential of the complementary information
- Precise localisation of organs and lesions
- Comparison of studies performed at different times

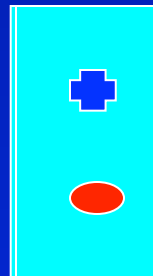
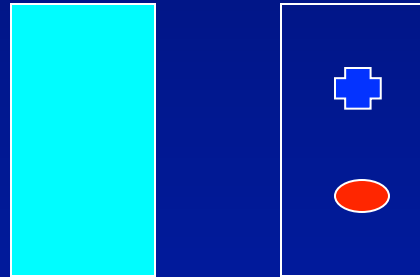
# Registration vs Fusion

- Registration = Technical manipulations applied to align images
- Fusion = Use of the registered images; most often superimposed images in a single display

# Registration



# Fusion



# How?

- Software used to identify the necessary transformation required, so that when it is applied to one study, the result is the best possible spatial alignment with another study
- Many different software packages available
- Many different ways to register images



# Transformations

- Rigid (Linear)
  - position or orientation different between two image sets
  - simple translation or rotation required
  - used to register scans from the same patient at different times

# Transformations

- Affine (Linear)
  - additional scaling/zooming and shearing
  - spatial transformation of one co-ordinate system (x,y,z) to another (u,v,w)

$$u = p_1x + p_2y + p_3z + p_4$$

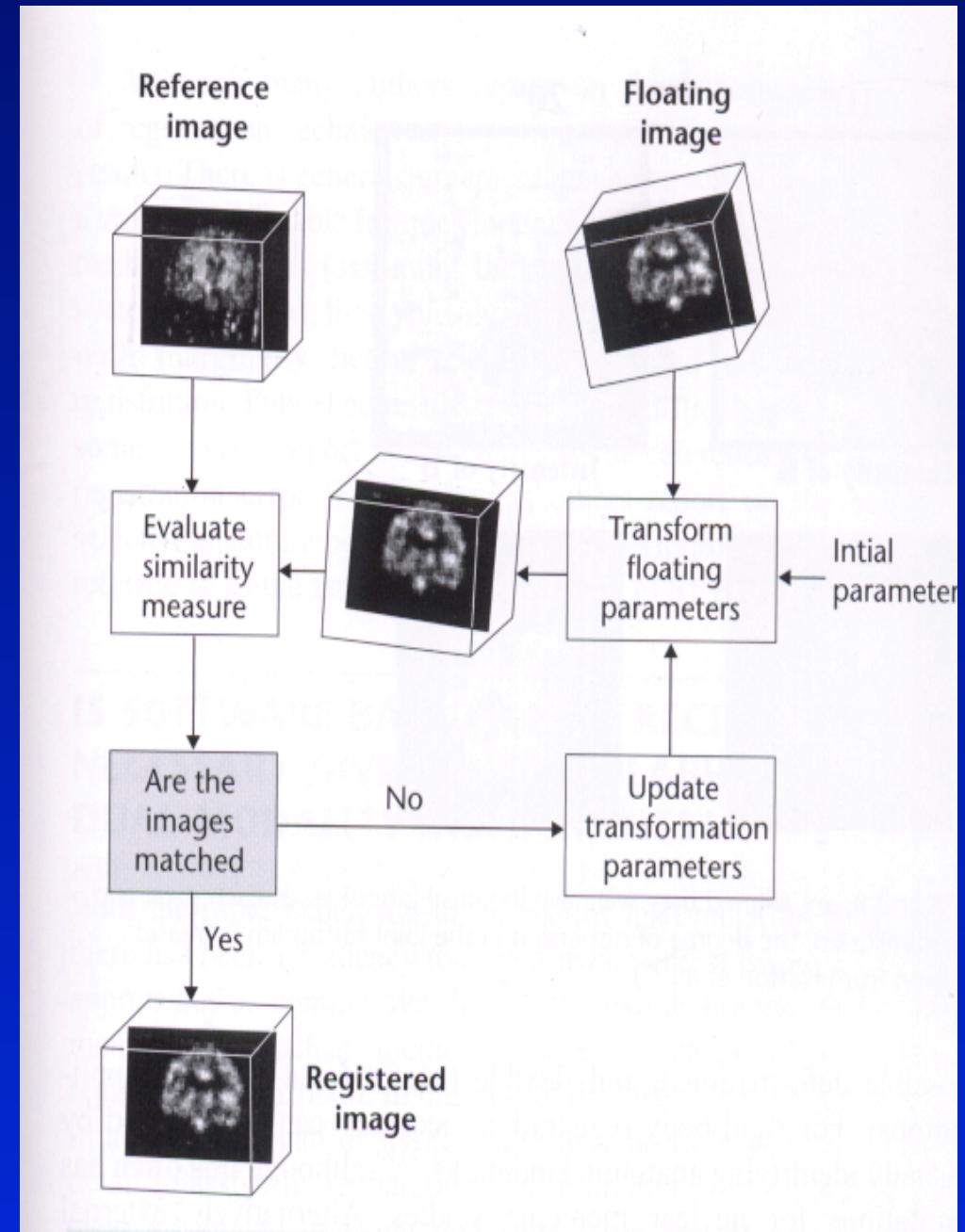
$$v = p_5x + p_6y + p_7z + p_8$$

$$w = p_9x + p_{10}y + p_{11}z + p_{12}$$

# Transformations

- Non-linear
  - usually applied after linear techniques
  - correct for differences in shape that cannot be accounted for by affine normalisation
  - warping of the image

- Initial guess at transformation parameters
- Floater reorientated
- Similarity compared
- Parameters updated
- Continued until preset termination point reached



# Measures of Similarity

- Require a quantitative measure of alignment between the two images
- Similarity measure will reach a maximum when the images are most closely aligned
- ‘Best match’ ambiguous
- Large variety been proposed

# Measures of Similarity

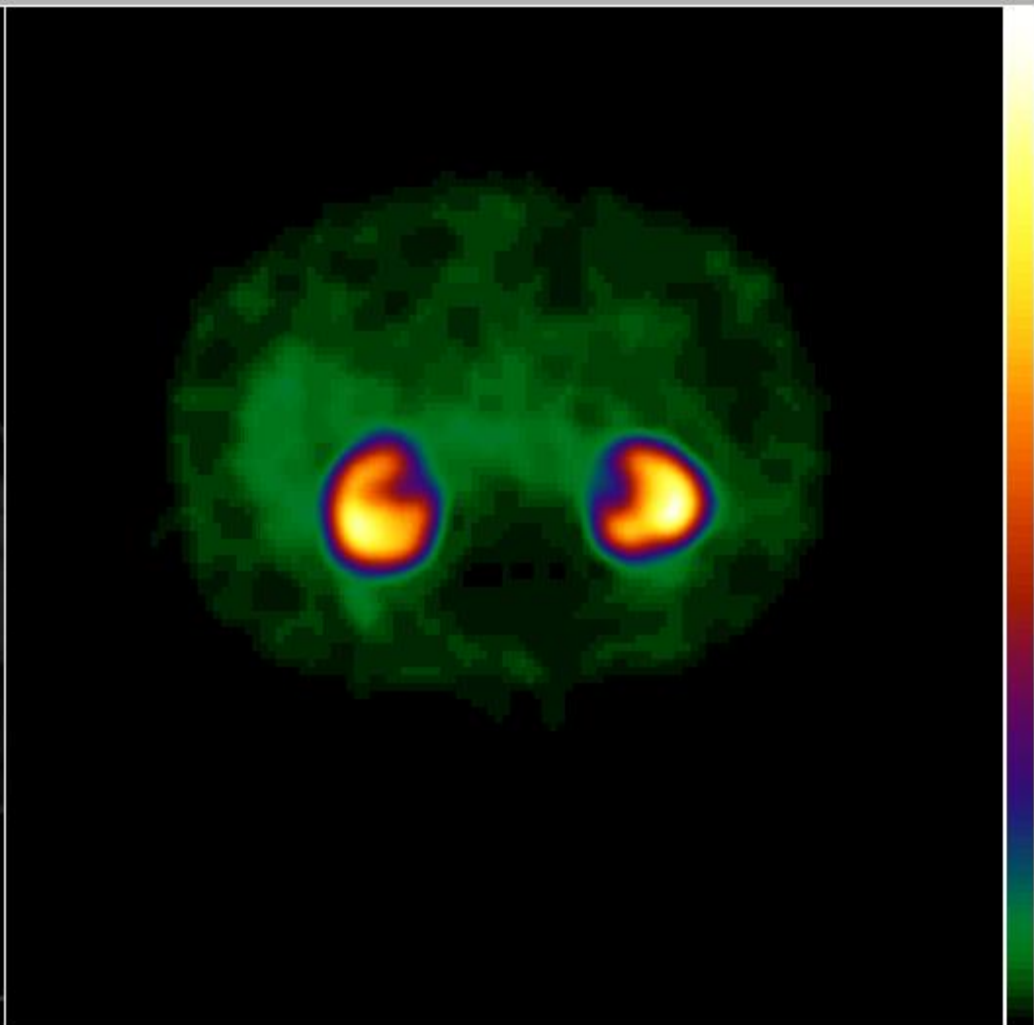
- Point based methods
  - extrinsic markers (prospective)
  - intrinsic markers (retrospective)
- Comparison of voxel intensity values
- Edge/Surface based

# Wrist Registration

- Splint with cobalt markers
- UV sensitive
- Digital DP film
- Registered with bone scan

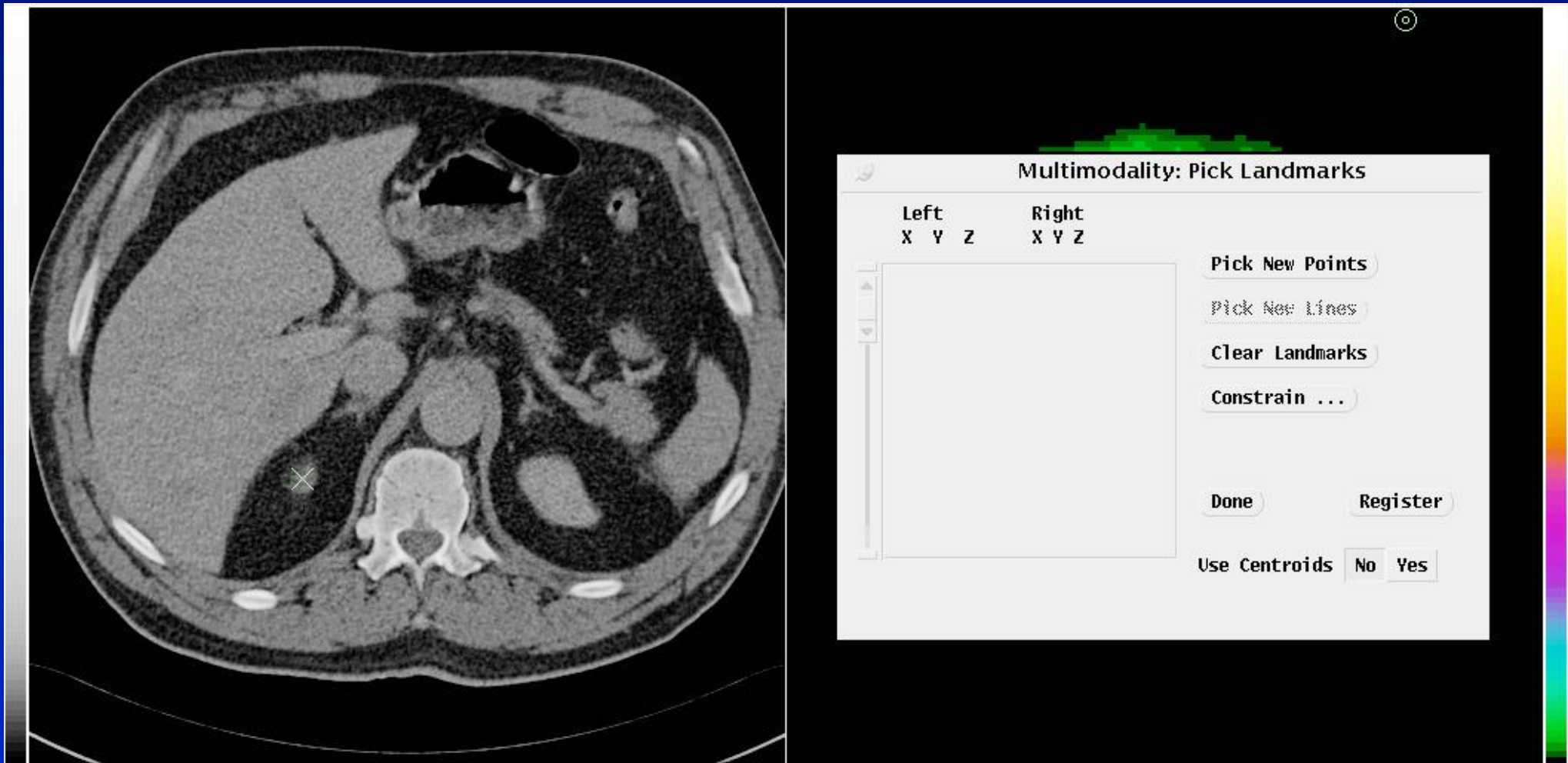


# Intrinsic Markers





# Intrinsic Markers



CT 11

Window 2239 0 4096

Max 862 0 1724

CT 2

Level 970 -1000 4096

Min 0 0 1724



Slice: 374

Slice: 374

Slice: 33



Landmark Mode

# Intrinsic Markers

Multimodality: Pick Landmarks

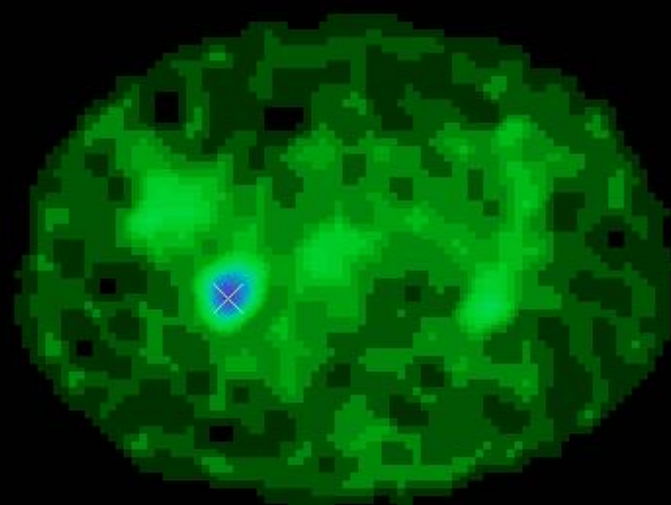
| Left |     |     | Right |    |   |
|------|-----|-----|-------|----|---|
| X    | Y   | Z   | X     | Y  | Z |
| 184  | 195 | 373 | 47    | 69 | 5 |

Pick New Points  
Pick New Lines  
Clear Landmarks  
Constrain ...

Done Register

Use Centroids  No  Yes

Nr of Landmarks: 1



CT 11

Window 2239 0 4096

Max 862 0 1724

CT 2



Slice: 6

Level 970 -1000 4096



Min 0 0 1724

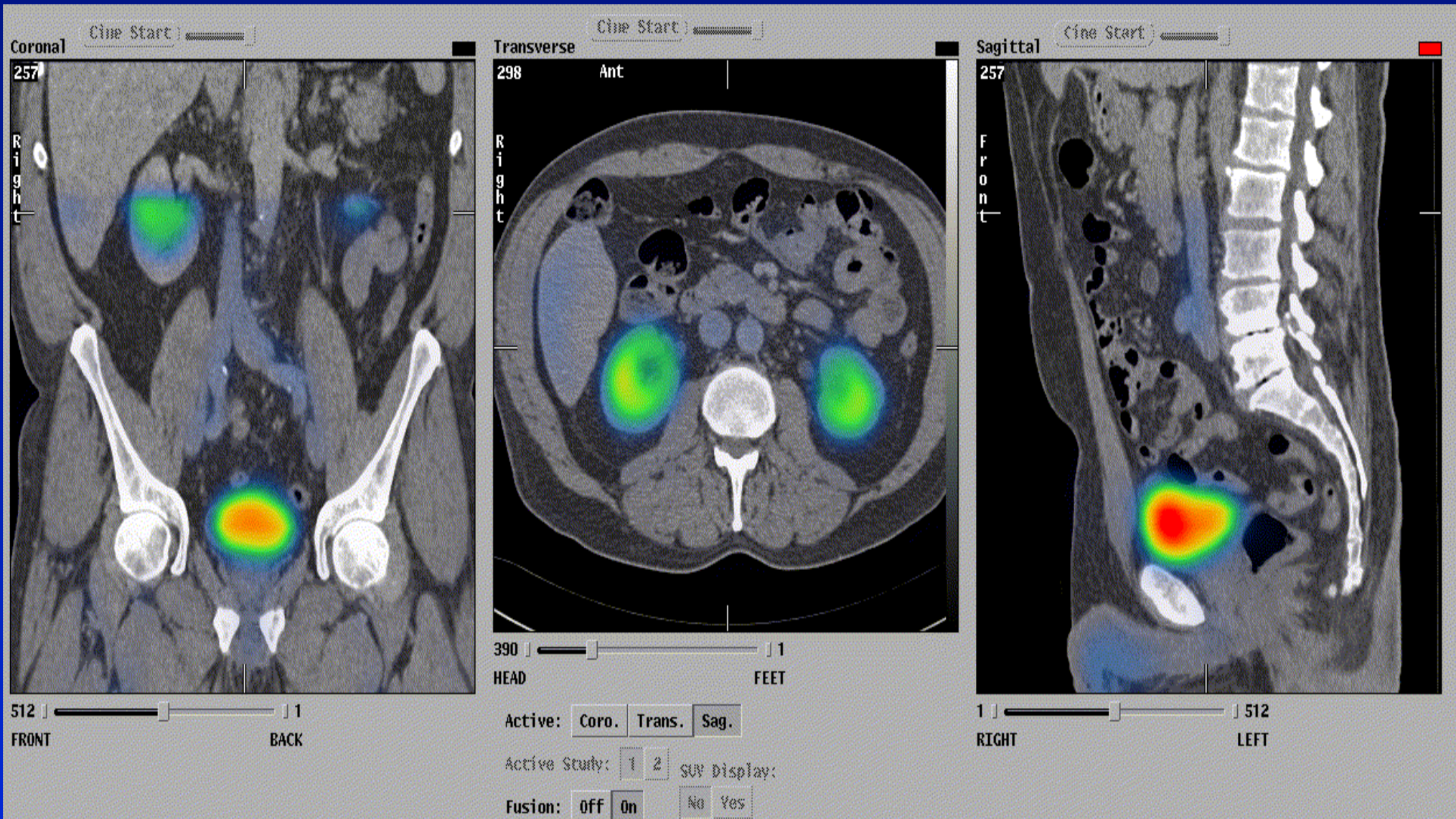
Slice: 6

Slice: 6



Landmark Mode

# Layout of fused images



# Image Display

- Fusion Display
  - Grey scale for CT/MR
  - Colour for PET/SPECT
  - New colour values computed for each pixel, simulating the transparency effect
  - Artificial increase in the perceived intensity of colour images

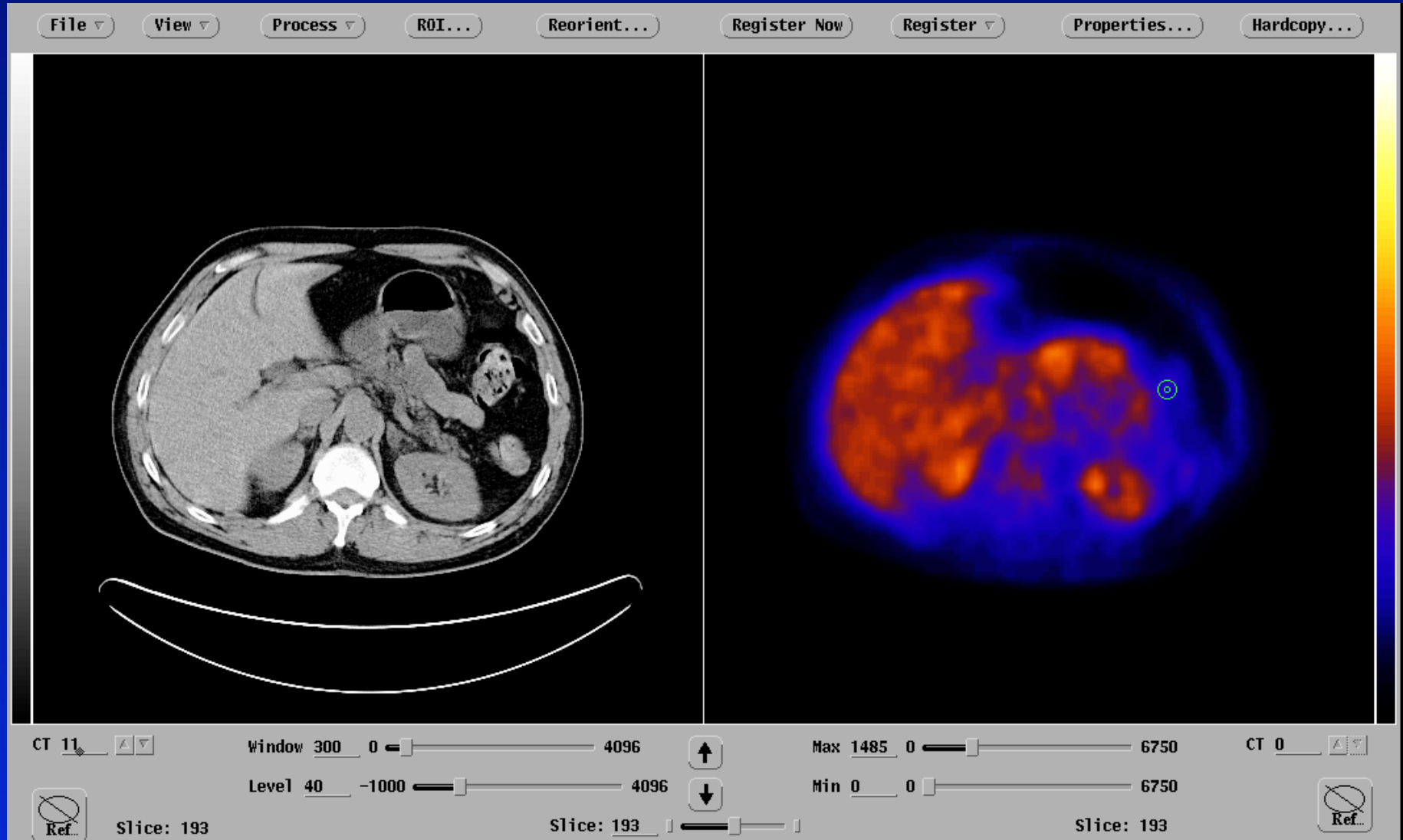
# Image Display

- Multimodality Display
  - Display both modalities side by side
  - Synchronized cursors displayed simultaneously on both images
  - Advantage no information lost

# Fused Display



# Multimodality Display



# <sup>99m</sup>Tc HMPAO images superimposed on MR images

NUD DEMO G A Brain 3D 1994-04-26      NUD DEMO G A CBF-HMPAO-C 1994-04-27

File View Process ROI... Reorient... Register Properties... Backup...

CT 12    Window 43    Level 28    UT 100    LT 0    CT 8

Slice: 38    Measurement: None    Slice: 38

**Left Reference Views**

KV tilt    VZ tilt

**Interactive Measurement**

|                      |          |       |             |
|----------------------|----------|-------|-------------|
| Distance (mm):       | 135.3    |       |             |
| X Y Z (mm):          | 92.0     | 190.0 | 0.0         |
| X Y Z (vessels):     | 168      | 173   | 37          |
| Value LEFT           | 2        | -     | 2 % of MAX  |
|                      |          |       | 25 % of REF |
| Angle to Horizontal: | 47.4 deg |       |             |
| Angle to Vertical:   | 42.6 deg |       |             |

Draw:

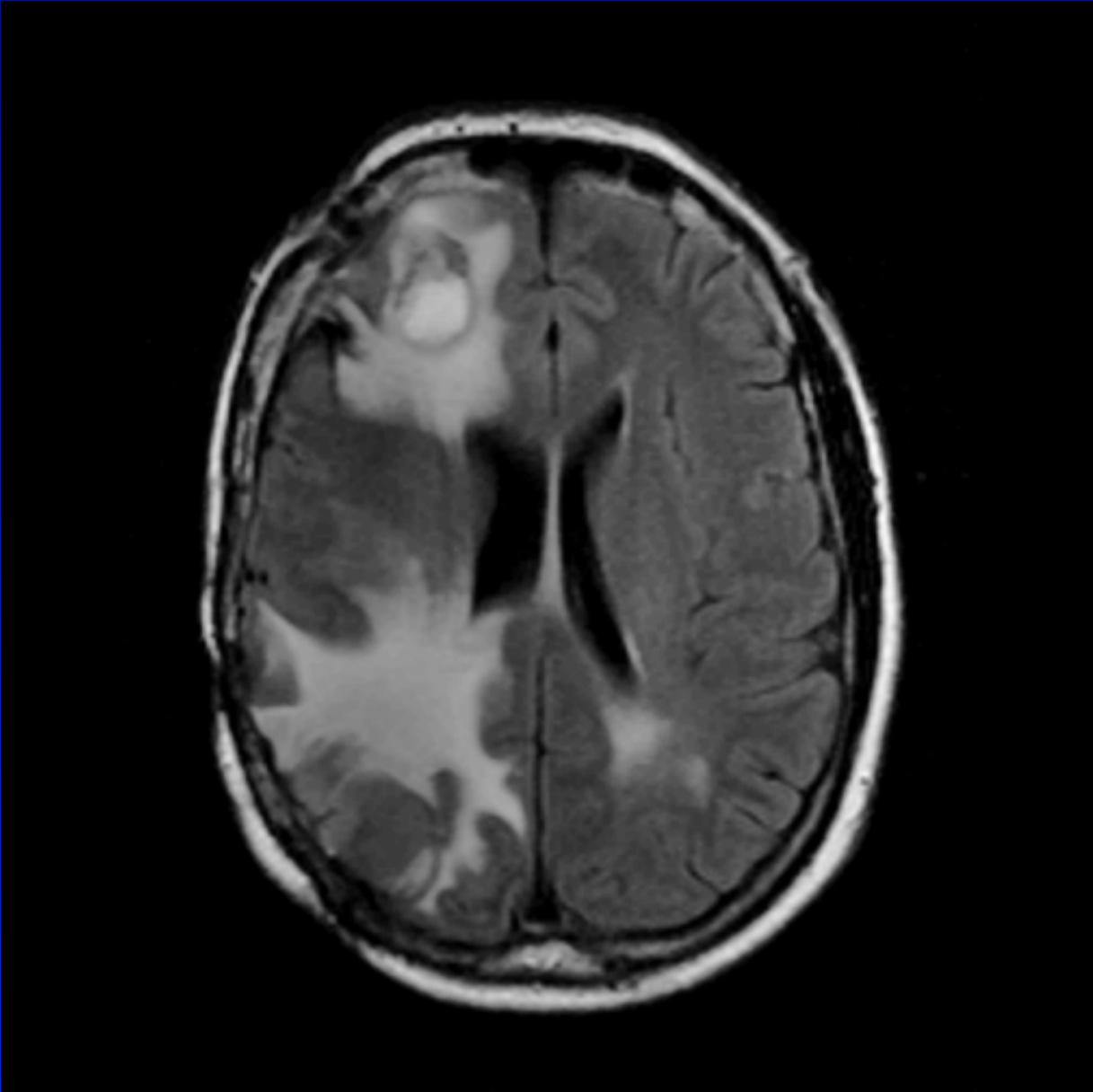
**Right Reference Views**

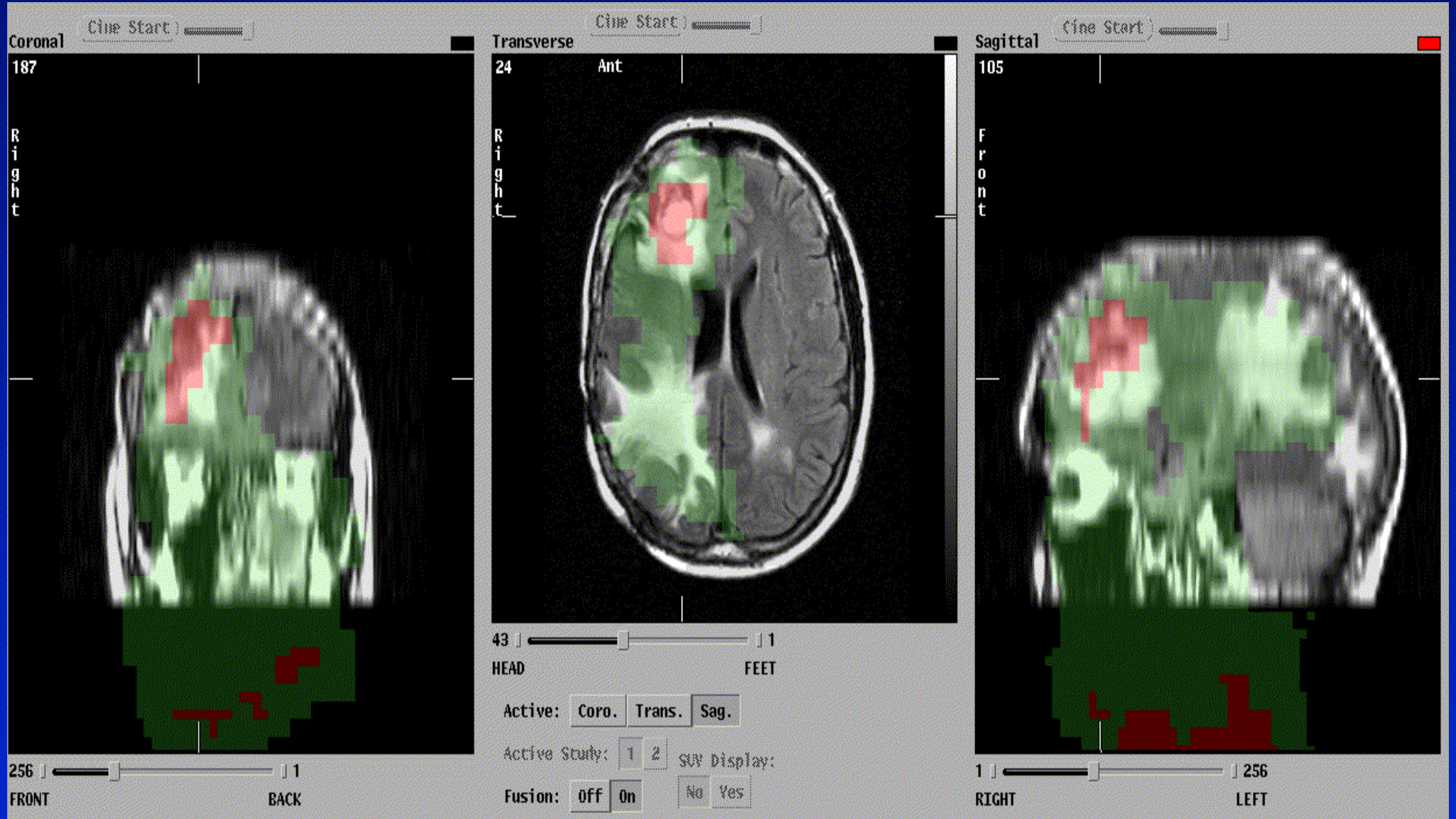
KV tilt    VZ tilt



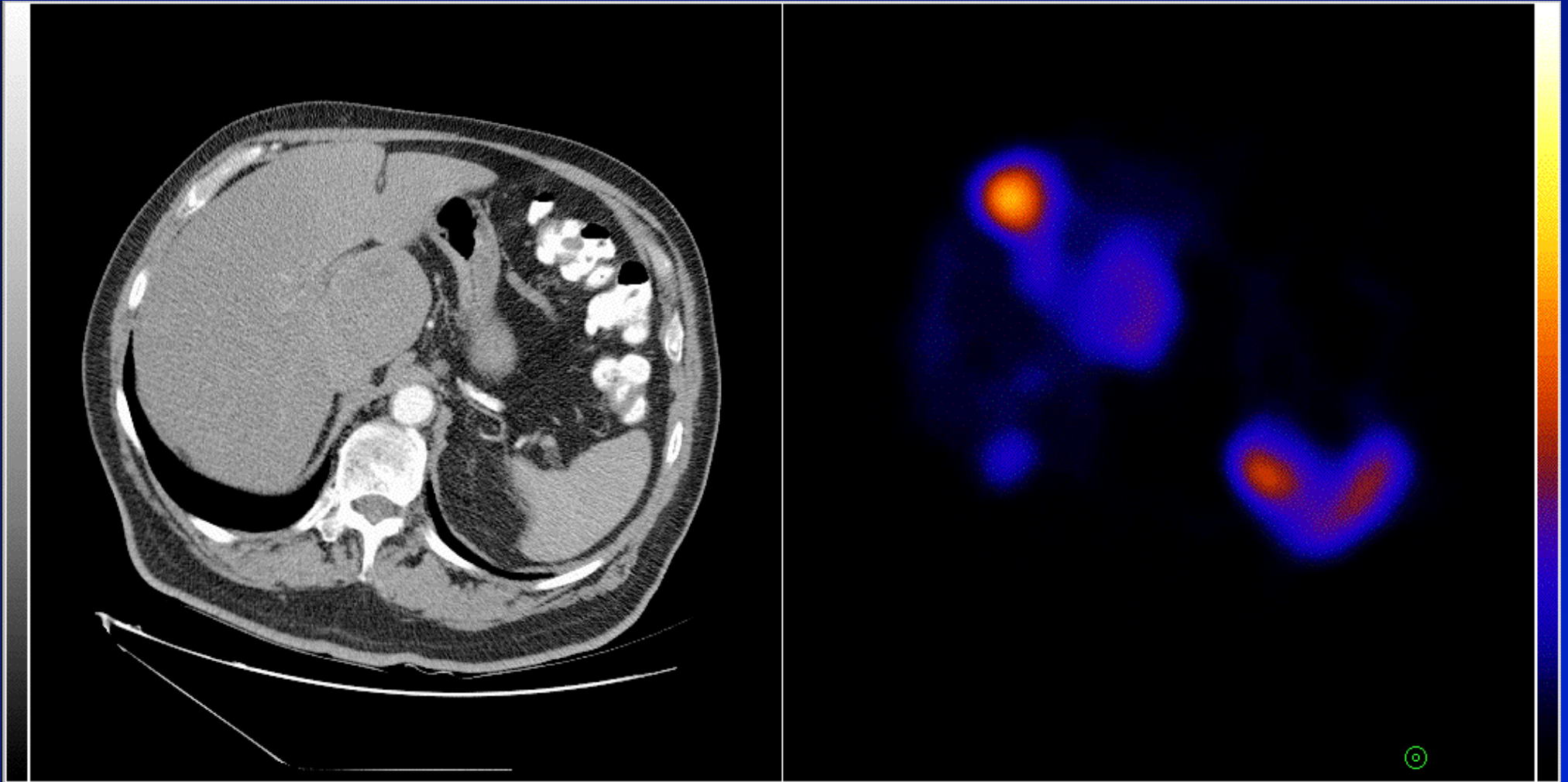
# Oncology - Clinical Applications

- Registration MR, CT, SPECT and PET
- Excellent tool in radiotherapy planning
- Biopsy guidance
- Surgical planning
- SPECT (with CEA, prostacint scans, targeted therapy, accurate lesion localisation)

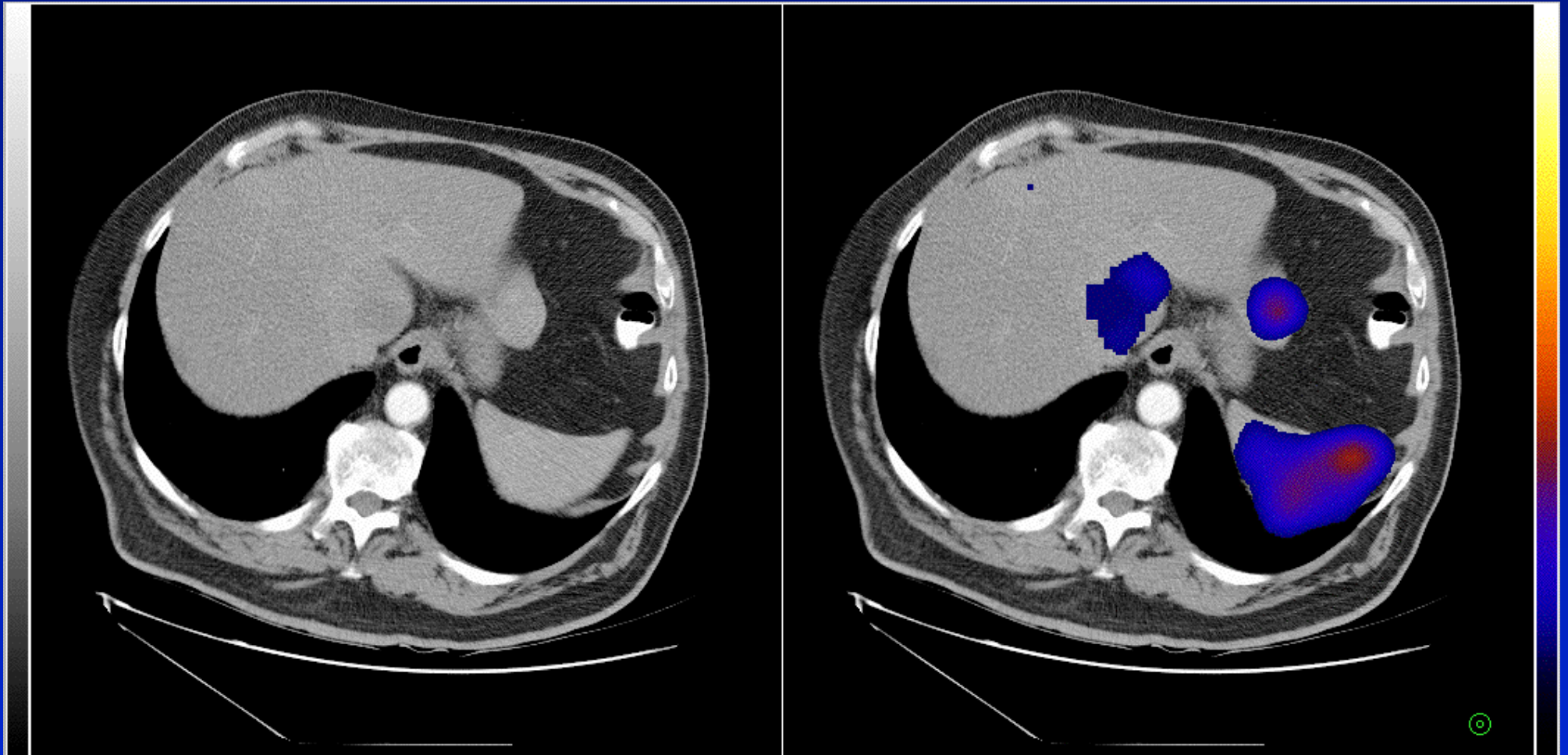




# SRS Registered



# SRS Fused

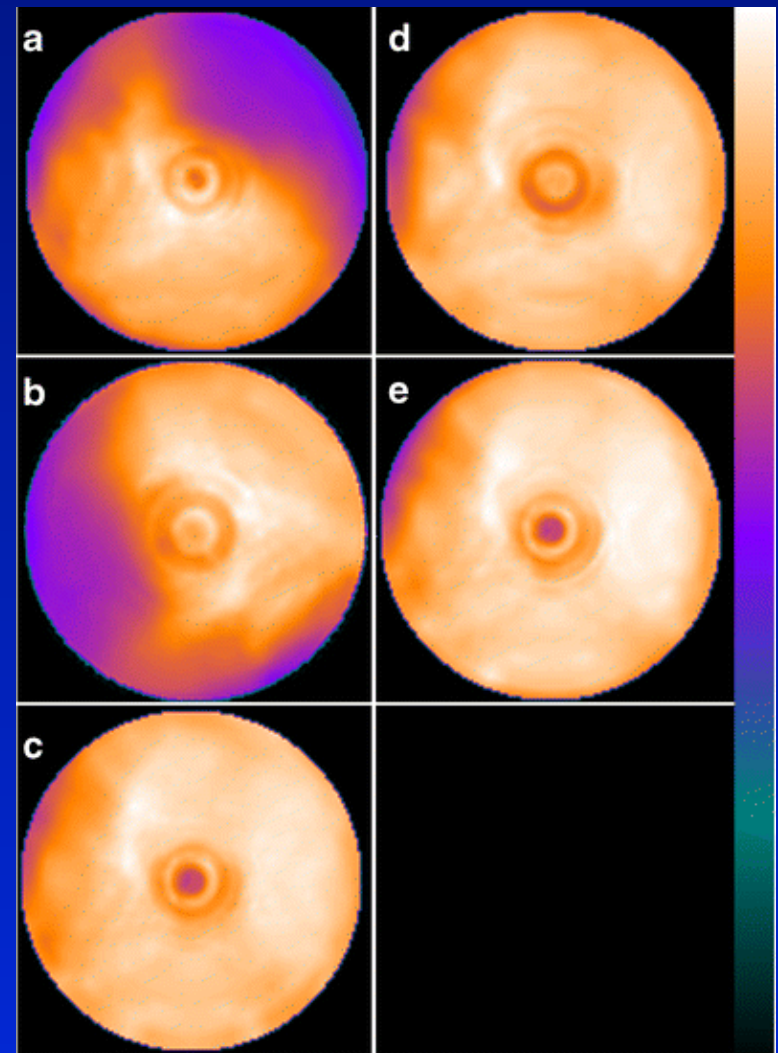


# Pitfalls and problems

- *Not unique to SPECT-CT but may be worse because of longer acquisition times*
- *Respiration and mis-registration and AC-errors in lower chest, liver and spleen*
- *Over correction around high density objects in iterative recon-suggest use back-projection*

# Effects of movement of chest

- *McQuaid and Hutton*  
*UCL, EANMMI*
- *a) cardiac mismatch*
- *b) heart and liver overlap*
- *c) lung movement-  
diaphragm*
- *d) lung movement chest  
wall*
- *e) correct image*



# Is it being used?

- Despite undoubted advantages, clinical applications limited
- Limitations
  - requires knowledge of registration methods
  - can be misused and is time consuming
  - very mathematical (involve a physicist)
  - easier with automated systems
  - movement (subject, diaphragm, cardiac)
  - organ changes (GB, bladder)



# In Summary

- Powerful, versatile and available tool
- Does have limitations and must be used with caution
- Clinical use of dedicated hardware and software registration will increase
- Software registration will remain important for hardware devices